

Imaging Sciences and Mathematics

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Imaging Sciences

- The *SIAM Journal on Imaging Sciences* covers all areas of imaging sciences, broadly interpreted. It includes
 - image formation (imaging)
 - image processing
 - image analysis
 - image interpretation and understanding
 - computer graphics and visualization
 - inverse problems in imaging;
- leading to applications to diverse areas in science, medicine, engineering, and other fields.



Imaging Sciences

- Image Acquisition (Imaging)
 - human vision, Optics, Radar imaging, Ultrasound, MRI, X-ray CT,...

- Image Processing

$$I_{input} \xrightarrow{T} I_{output} = T[I_{input}]$$

- Image Interpretation (Visual Intelligence)

Image Processing

- **What is Image?**
- **What is Image Enhancement?**
 - **Contrast Enhancement**
 - **Image Denoising**
 - **Image Deblurring**
- **Image Inpainting**
- **Image segmentation**
- **Image Registration**

Book: Rafael C. Gonzalez and Richard E. Woods,
[Digital Image Processing](#), Prentice Hall

What are Digital Images?

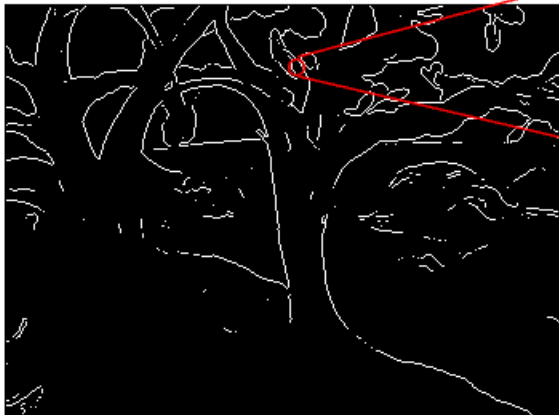
1. What is a digital image?

$$I : \Omega \rightarrow R \xrightarrow{\text{sampling, quantized}} I_d : \{1 \leq i \leq m, 1 \leq j \leq n\} \rightarrow R_k, 1 \leq k \leq l$$

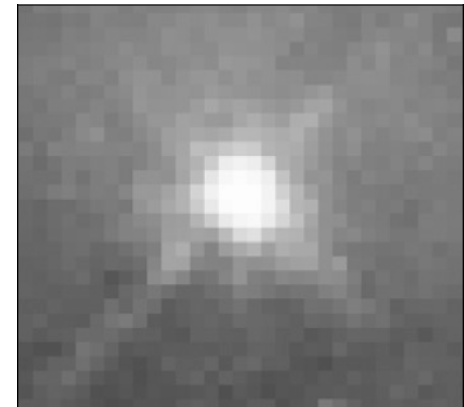
A digital image is an array, or a matrix, of square pixels (picture elements) arranged in columns and rows.

a. Binary Image (logical array)

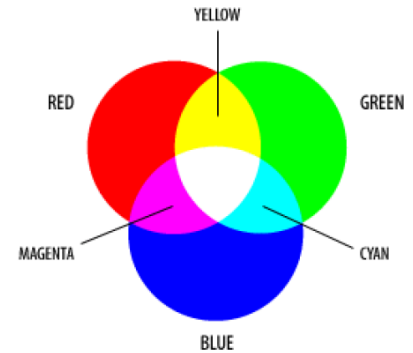
$$I(i, j) = \{1 \text{ or } 0\}$$



0	0	0	0	0	1
0	0	0	0	0	1
0	1	0	0	1	0
0	0	1	0	1	0
0	0	0	1	1	0
0	0	0	0	0	0



What are Digital Images?



b. Intensity Image

8 bit (uint8, 0-255), 16 bit (uint16, 0-65535) and double ([0 1])

c. color Image

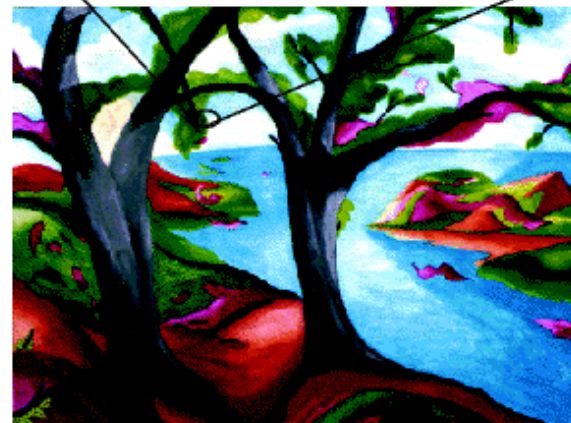
RGB:

24 bit = $256^3 \sim 16$ million colors

0.2251	0.2563	0.2826	0.2826	0.4		
0.5342	0.2051	0.2157	0.2826	0.3822	0.4391	0.4391
0.5342	0.1789	0.1307	0.1789	0.2051	0.3256	0.2483
0.4308	0.2483	0.2624	0.3344	0.3344	0.2624	0.2549
0.3344	0.2624	0.3344	0.3344	0.33		



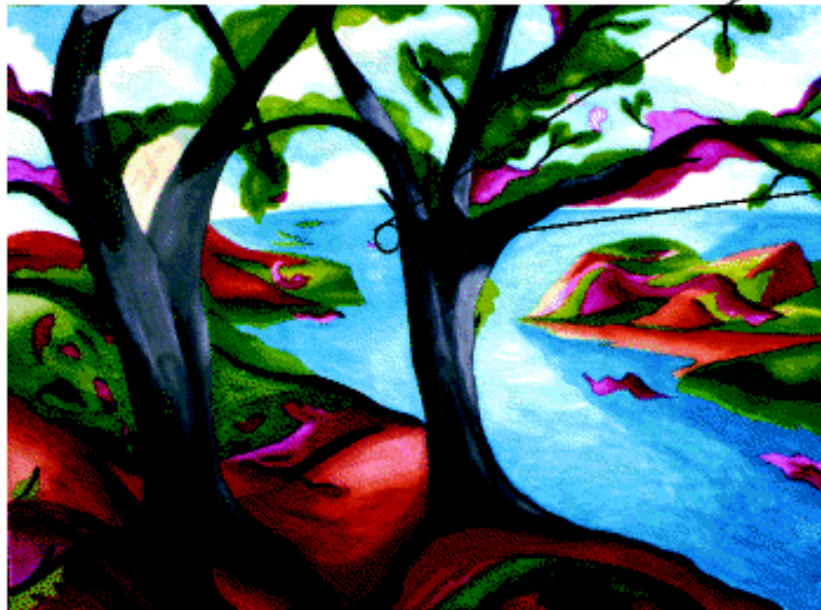
0.5804	0.2235	0.1294	Blue	0.4196		
0.5804	0.2902	0.0627	0.2902	0.2902	0.4824	
0.5804	0.0627	0.0627	0.0627	0.2235	0.2588	
0.5176	0.1922	0.0627	Green	0.1922	0.2588	0.2588
0.5176	0.1294	0.1608	0.1294	0.1294	0.2588	0.2588
0.5176	0.1608	0.0627	0.1608	0.1922	0.2588	0.2588
0.5490	0.2235	0.5490	Red	0.7412	0.7765	0.7765
0.5490	0.3882	0.5176	0.5804	0.5804	0.7765	0.7765
0.5490	0.2588	0.2902	0.2588	0.2235	0.4824	0.2235
0.5490	0.2235	0.1608	0.2588	0.2588	0.1608	0.2588
0.5490	0.2588	0.1608	0.2588	0.2588	0.2588	0.2588



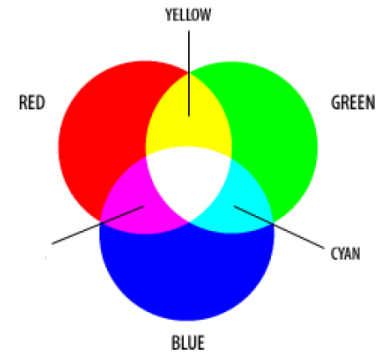
What are Digital Images?

c. index color Image

data matrix and colormap matrix



12	21	40				
14	17	21	21	53	53	
5	8	5	8	10	30	15
15	18	31	31	18	16	
18	31	31	31			
0	0	0				
0.0627	0.0627	0.0314				
0.2902	0.0314	0				
0	0	1.0000				
0.2902	0.0627	0.0627				
0.3882	0.0314	0.0941				
0.4510	0.0627	0				
0.2588	0.1608	0.0627				
	⋮					



Examples of images

- Daily-life images
- Astro images
- Medical images

Standard images



No higher resolution available.

Lenna.png (512 × 512 pixels, file size: 464 KB, MIME type: image/png)

Hubble site

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Hubble images become large-scale artwork for your home. Have these photographs



3D-DOCTOR

3D-DOCTOR

FDA 510K CLEARED, VECTOR-BASED 3D IMAGING, MODELING AND MEASUREMENT SOFTWARE

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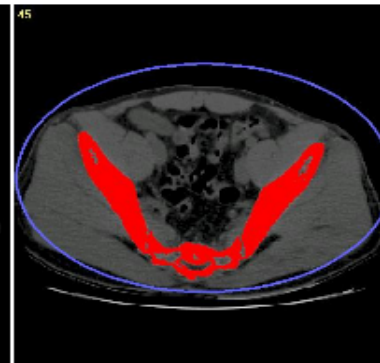
[User List](#)

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"3D-DOCTOR Software has been one of the tremendous analysis software that I use on a regular bases to extract information from image files to create 3D model.", A. Udoh, R&D Design Systems



Step 1. Original CT image



Step 2. Segmentation



Step 3. 3D mesh model created

[3D-DOCTOR](#) is an advanced 3D modeling, image processing and measurement software for MRI, CT, PET, microscopy, scientific, and industrial imaging applications.

Image Processing

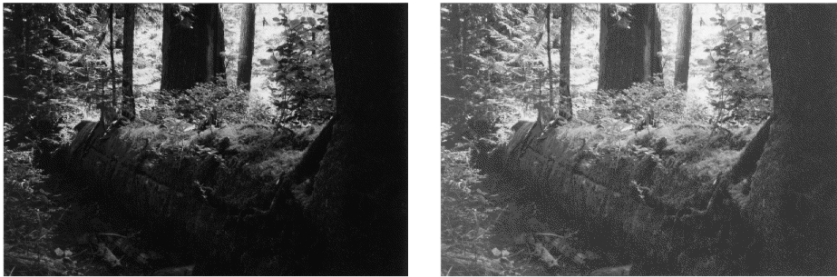
- **What is Image?**
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Image Enhancement

1. Image Enhancement

a. Intensity Adjustment



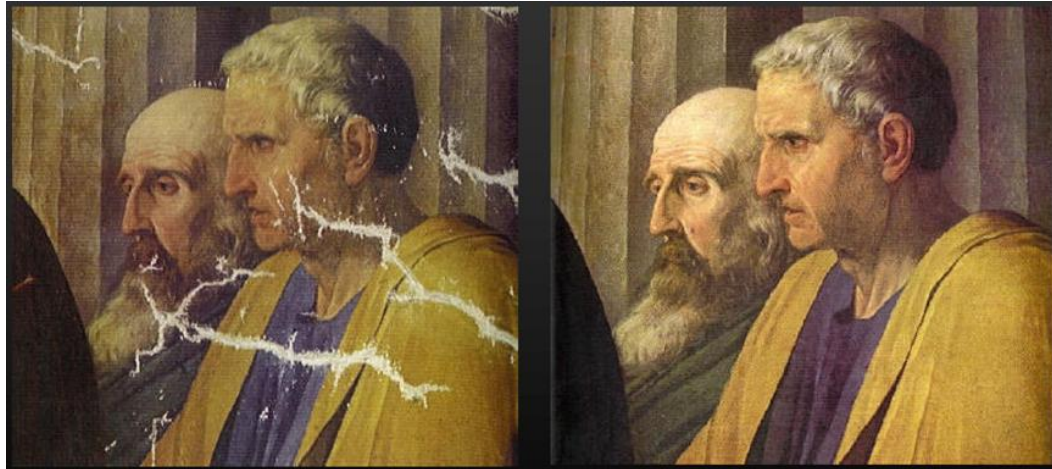
b. Denoise



c. Deblur



Image Inpainting



***“Image Inpainting :
An Overview”***,
Guillermo Sapiro

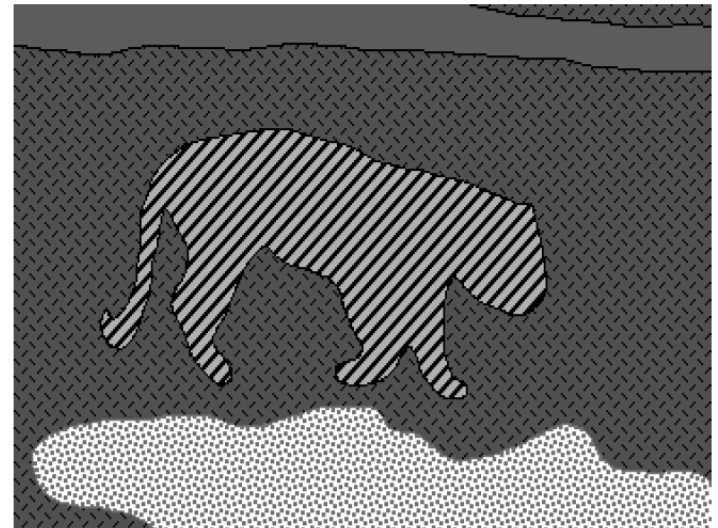


***“Fast Digital
Image Inpainting”***,
Manuel M. Oliveira,
Brian Bowen,
Richard McKenna
and Yu-Sung Chang

Introduction to Image Segmentation

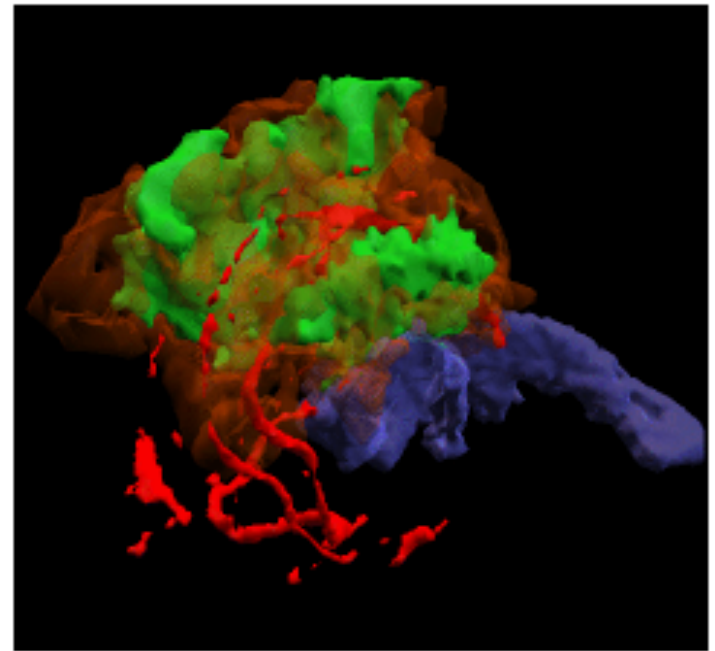
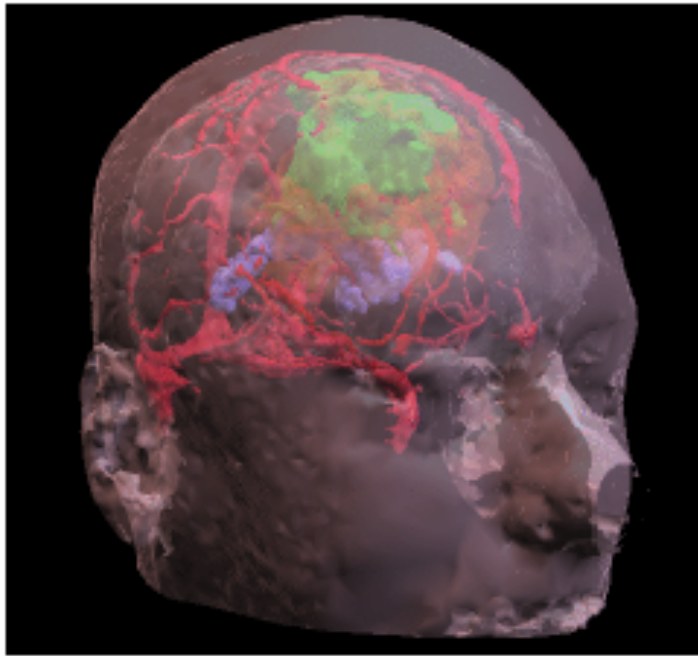
Chiu-Yen Kao

$$X = \bigcup_{i=1}^N R_i, R_i \cap R_j = 0 \text{ for } i \neq j$$



Chiu-Yen Kao

Image Registration



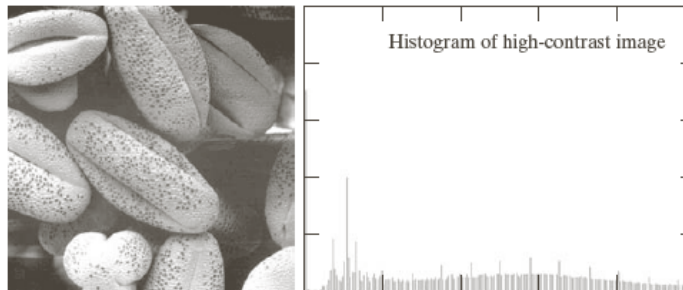
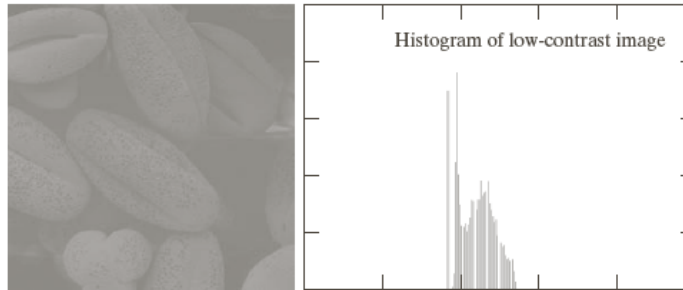
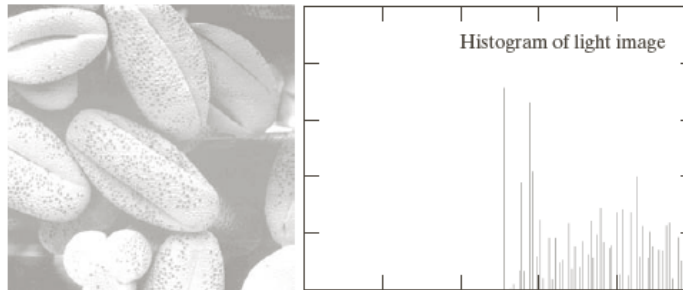
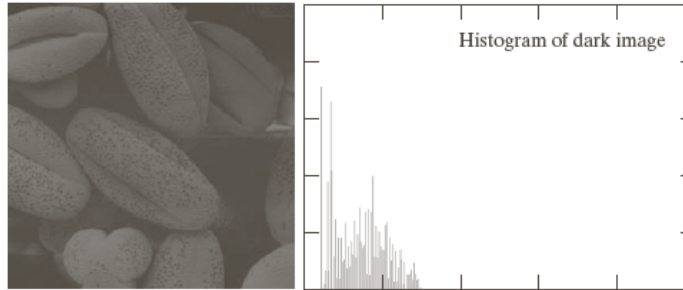
Tumor(green), Vessels(red), Ventricles(blue), Edema (orange)

Image Processing

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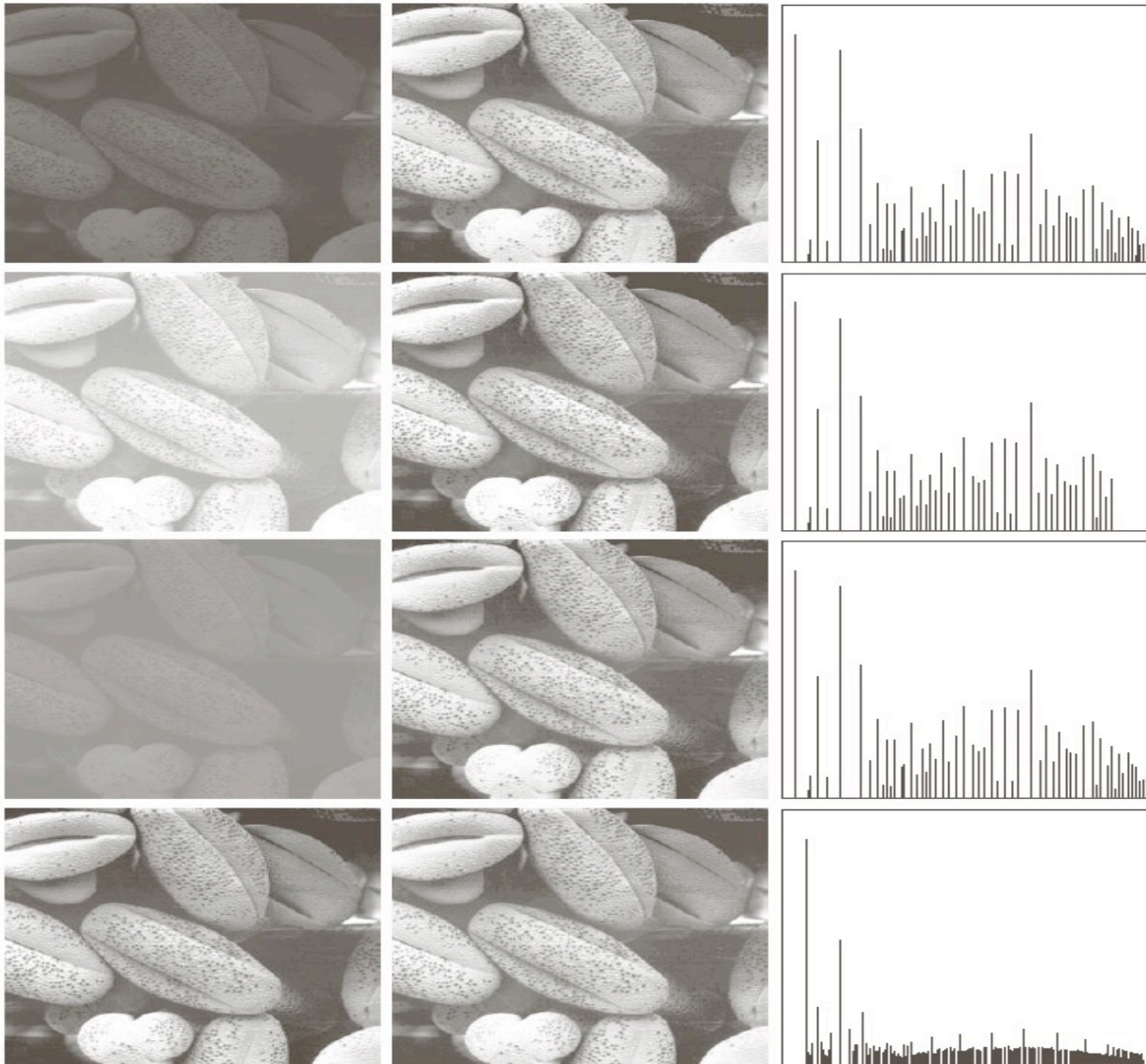
Book: Rafael C. Gonzalez and Richard E. Woods,
[Digital Image Processing](#), Prentice Hall

Contrast enhancement-1



Histogram

Contrast enhancement-2

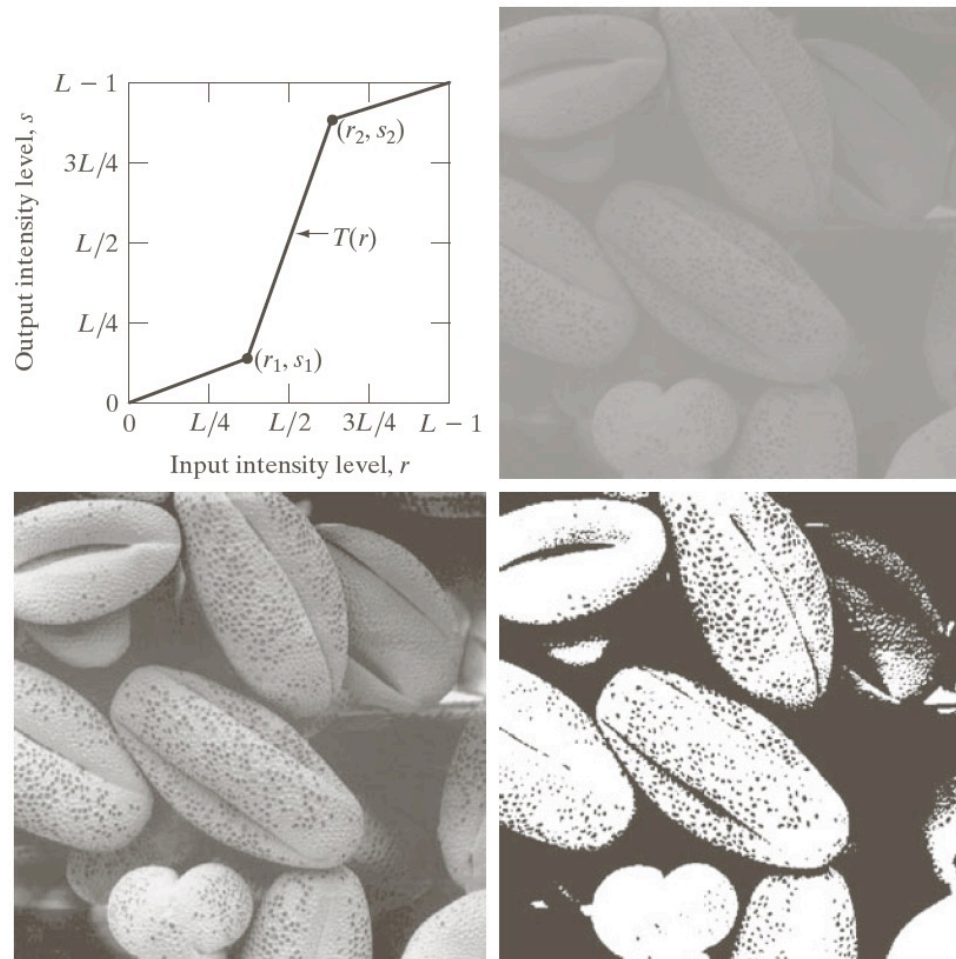


Histogram
equalization

$$g(x, y) = T[f(x, y)]$$

Contrast Enhancement -3

- Gray-level transform $g(x, y) = T[f(x, y)]$



a	b
c	d

FIGURE 3.10
Contrast stretching. (a) Form of transformation function. (b) A low-contrast image. (c) Result of contrast stretching. (d) Result of thresholding. (Original image courtesy of Dr. Roger Heady, Research School of Biological Sciences, Australian National University, Canberra, Australia.)

Image Processing

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Noise models

- Assume white noise

$n(x, y)$ and $n(x', y')$ are uncorrelated

- Types of noises

- Additive noise

$$g = f + n, \quad n : \text{mean } 0, \text{ variance } \sigma^2$$

- Multiplicative noise

$$g = fn, \quad n : \text{mean } 1, \text{ variance } \sigma^2$$

- Mixed

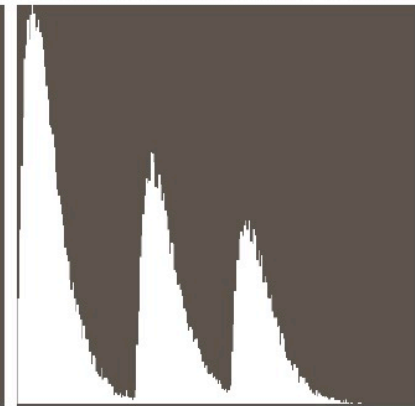
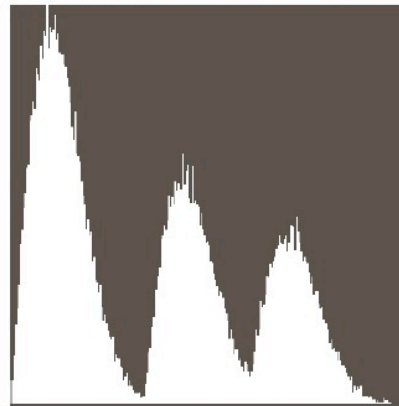
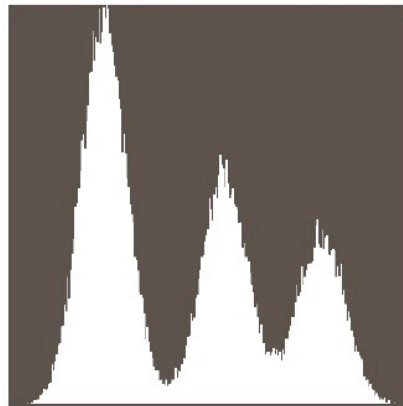
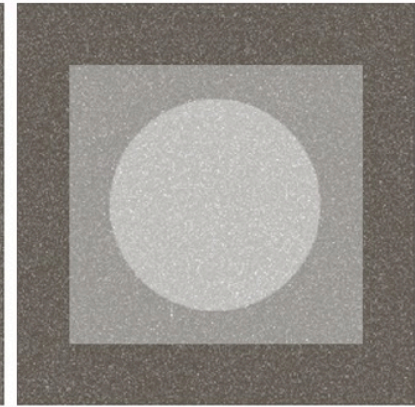
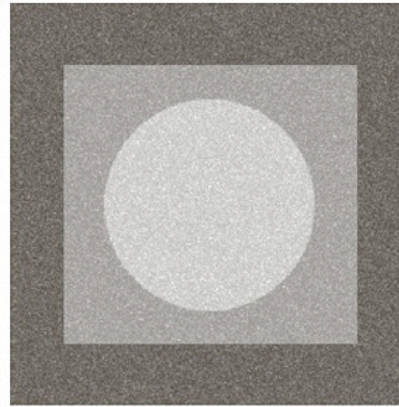
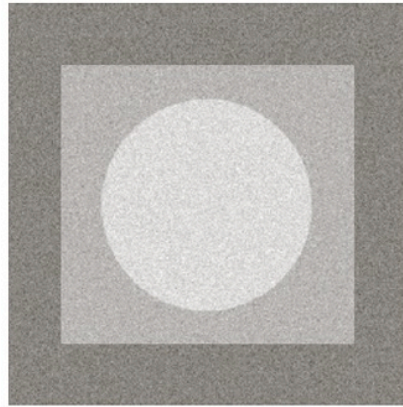
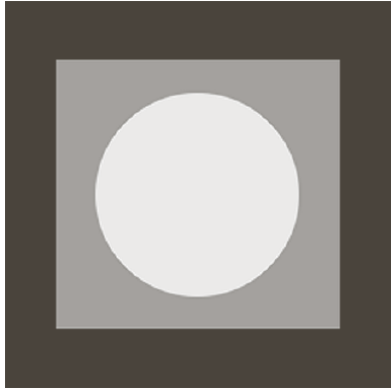
$$g = fn_1 + n_2$$

Noise Models-2

Gaussian

Rayleigh

Gamma



$$g = f + n$$

Gaussian

Rayleigh

Gamma

a	b	c
d	e	f

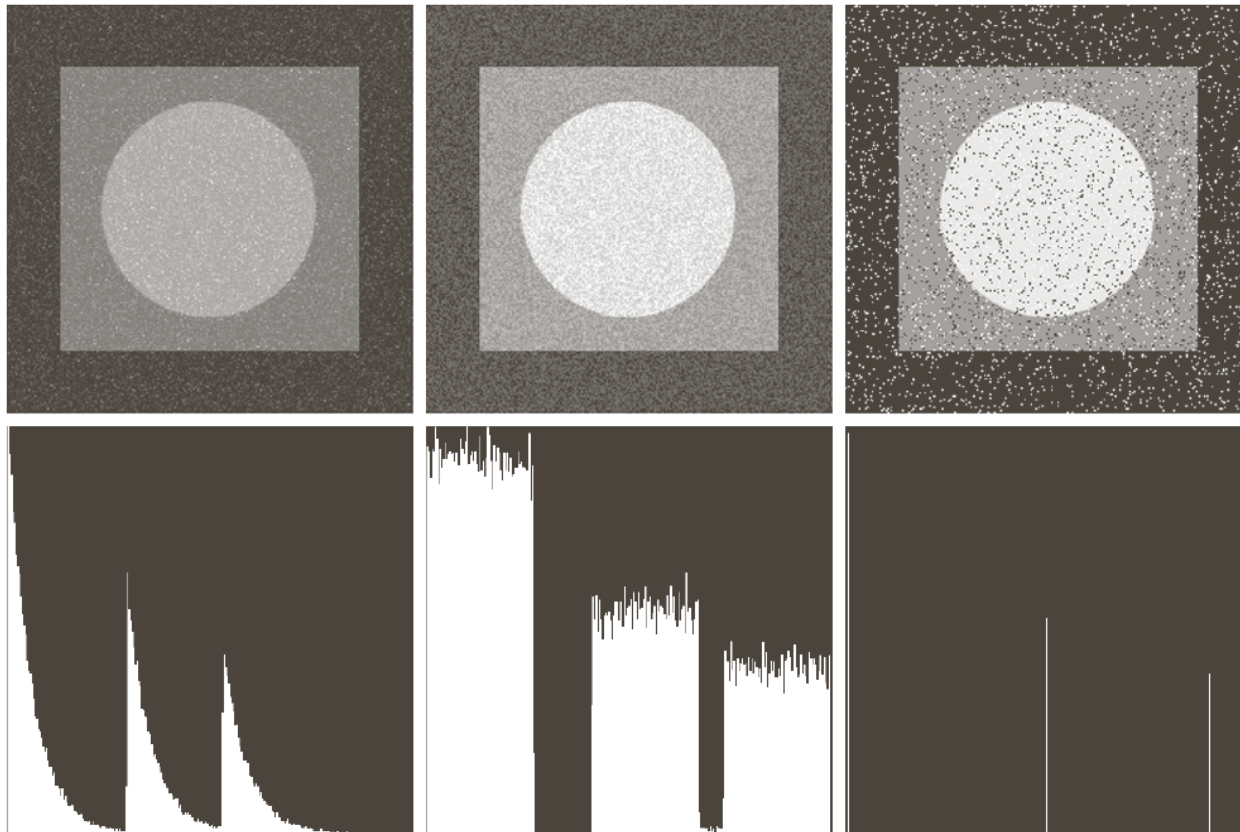
FIGURE 5.4 Images and histograms resulting from adding Gaussian, Rayleigh, and gamma noise to the image in Fig. 5.3.

Noise Models-3

Exponential

Uniform

Salt & Pepper



Exponential

Uniform

Salt & Pepper

g h i
j k l

FIGURE 5.4 (Continued) Images and histograms resulting from adding exponential, uniform, and salt and pepper noise to the image in Fig. 5.3.

Denoise methods

- Filtering techniques
 - Spatial filtering
 - Mean filters
 - Order-Statics filters
 - Frequency filtering
 - Wavelet filtering
- Variational approach

Spatial filtering

- Mean filters:
 - Arithmetic mean filter
 - Geometric mean filter
 - Harmonic mean filter

$$g = f + n$$

$$\tilde{f}(x, y) = \frac{1}{mn} \sum_{(s,t) \in S_{x,y}} g(s, t)$$

$$g = fn$$

$$\tilde{f}(x, y) = \left[\prod_{(s,t) \in S_{x,y}} g(s, t) \right]^{\frac{1}{mn}}$$

$$\tilde{f}(x, y) = \frac{mn}{\sum_{(s,t) \in S_{x,y}} \frac{1}{g(s, t)}}$$

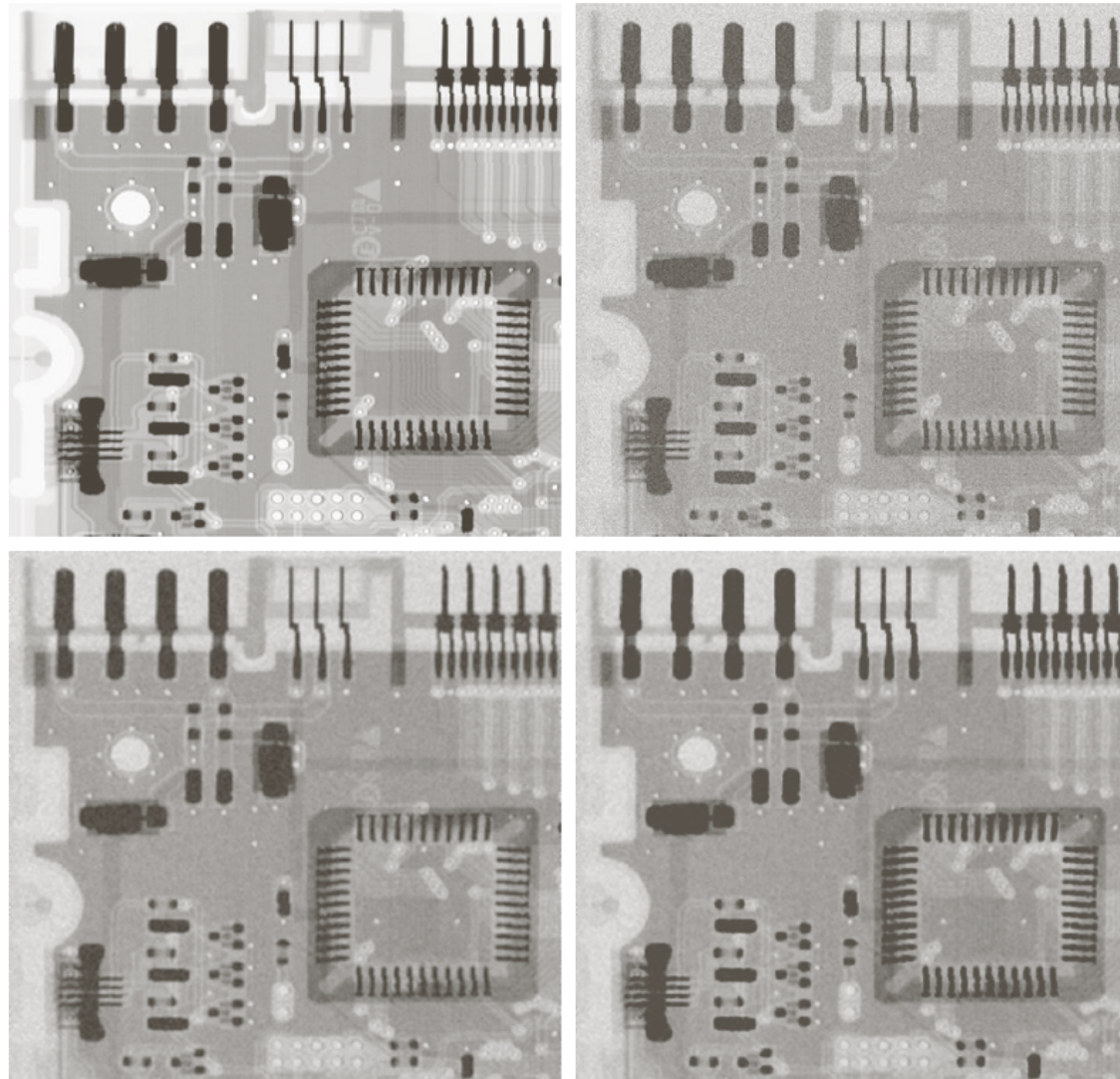
Mean filterings

a	b
c	d

FIGURE 5.7

(a) X-ray image.
(b) Image corrupted by additive Gaussian noise.
(c) Result of filtering with an arithmetic mean filter of size 3×3 .
(d) Result of filtering with a geometric mean filter of the same size.

(Original image courtesy of Mr. Joseph E. Pascente, Lixi, Inc.)



Mean filtering

- Convolution with a smoothing mask

$$\tilde{f}_{i,j} = h * g := \sum_{|s|,|t|\leq 1} h_{s,t} g_{i-s,j-t}$$

$$\frac{1}{16}$$

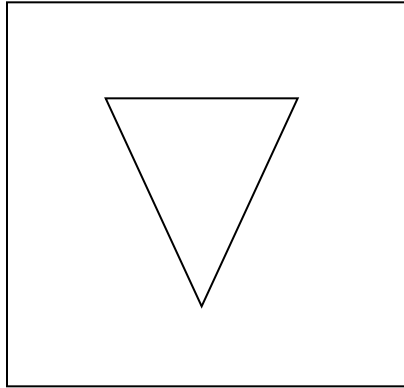
1	2	1
2	4	2
1	2	1

$$h_{s,t}$$

Denoise methods

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Impulse Noise Model



Original Image
(a triangle)

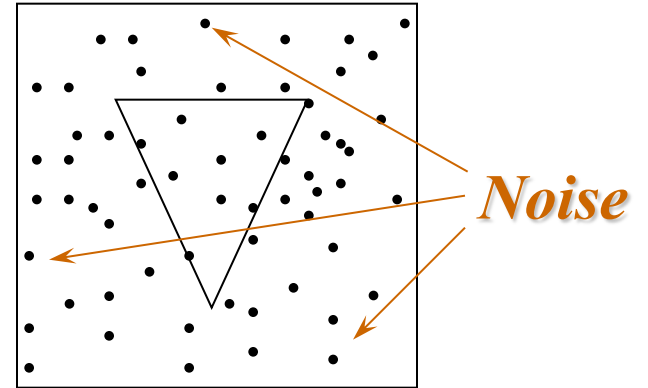


Image corrupted
by *Impulse Noise*

Only a number of pixels are corrupted

Impulse Noise Model

Impulse Noise are caused by

- ❑ **Malfunctioning pixels** in camera sensors
- ❑ **Faulty memory locations** in hardware
- ❑ **Transmission** in a noisy channel

Two types of Impulse Noise

- I. Salt-and-Pepper Noise
- II. Uniformly-Distributed Random Noise

Salt-and-Pepper Noise

$\mathbf{x} = (x_{i,j})$: true image with $x_{i,j} \in [0, 255]$.

$\mathbf{y} = (y_{i,j})$: observed noisy image.

$$y_{i,j} = \begin{cases} 0 & \text{with probability } r/2\%, \\ 255 & \text{with probability } r/2\%, \\ x_{i,j} & \text{with probability } 1 - r\%. \end{cases}$$

Noise level = $r\%$.



Noise-free Image



At 10% Noise



At 30% Noise



At 50% Noise

Random-Valued Impulse Noise

$\mathbf{x} = (x_{i,j})$: true image with $x_{i,j} \in [0, 255]$.

$\mathbf{y} = (y_{i,j})$: observed noisy image.

$$y_{i,j} = \begin{cases} n_{i,j} & \text{with probability } r, \\ x_{i,j} & \text{with probability } 1 - r, \end{cases}$$

where $n_{i,j}$ is randomly distributed in $[0, 255]$.

Denoising Schemes

Median Filter

Noisy Image

Restored Image

$y_{i-1,j-1}$	$y_{i-1,j}$	$y_{i-1,j+1}$	$y_{i-1,j-1}$	$y_{i-1,j}$	$y_{i-1,j+1}$
$y_{i,j-1}$	$y_{i,j}$	$y_{i,j+1}$	$y_{i,j-1}$	y_{i5}	$y_{i,j+1}$
$y_{i+1,j-1}$	$y_{i+1,j}$	$y_{i+1,j+1}$	$y_{i+1,j-1}$	$y_{i+1,j}$	$y_{i+1,j+1}$

Sort

Recovered

$$y_{i_1} \leq y_{i_2} \leq y_{i_3} \leq y_{i_4} \leq y_{i_5} \leq y_{i_6} \leq y_{i_7} \leq y_{i_8} \leq y_{i_9}$$

Median

30% Salt-and-Pepper Noise



Median filter

Median-type Filters

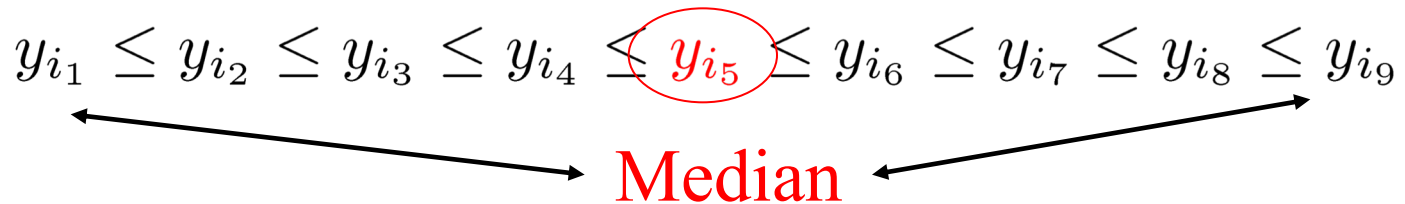
- ❑ Drawback of Median Filter: Every pixel is modified, hence **fuzziness** and **blurring**
- ❑ Extensions of Median Filters (**Median-type Filters**):
 - ❑ **Adaptive Median Filter** (Wang, *IEEE Trans IP*, (1995))
 - ❑ **Adaptive Center Weighted Median Filter** (2001)
 - ❑ **Multi-state Median Filters** (2001)
 - ❑ **Filter based on homogeneity info** (2003)
 - ❑ ...
 - ❑ **Detection statistics** (*IEEE TIP* 2007)

Adaptive Median Filter

Noisy Image

$y_{i-1,j-1}$	$y_{i-1,j}$	$y_{i-1,j+1}$
$y_{i,j-1}$	$y_{i,j}$	$y_{i,j+1}$
$y_{i+1,j-1}$	$y_{i+1,j}$	$y_{i+1,j+1}$

Sort



If **Median** = y_{i_1} or y_{i_9} , then increase window size.

Characteristics of Median-type Filters

Two Steps

- 1. Noise Detection* (e.g., thresholding)
- 2. Noise Replacement* (by **Median** or its variants)

Advantages

- 1. Fast*
- 2. Accurate Detection*

30% Salt-and-Pepper Noise



**Median
Filter**



**Adaptive
Median Filter**

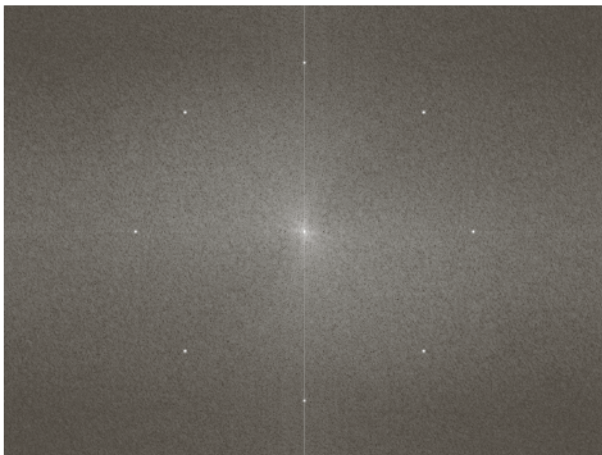
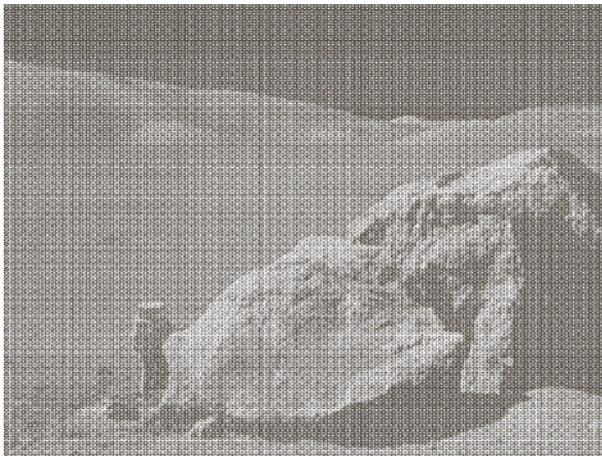


Denoise methods

- Filtering techniques
 - Spatial filtering
 - Mean filters
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 - Frequency filtering
- Variational approach

Frequency filter

- Noise in frequency



a
b

FIGURE 5.5

(a) Image corrupted by sinusoidal noise.
(b) Spectrum (each pair of conjugate impulses corresponds to one sine wave).
(Original image courtesy of NASA.)

Frequency filtering

- Taking Fourier transform:

$$\hat{f}(\xi, \eta) = \iint f(x, y) e^{-i(x\xi + y\eta)} dx dy$$

- Noise model:

$$\hat{g} = \hat{f} + N$$

- Band reject/pass filter

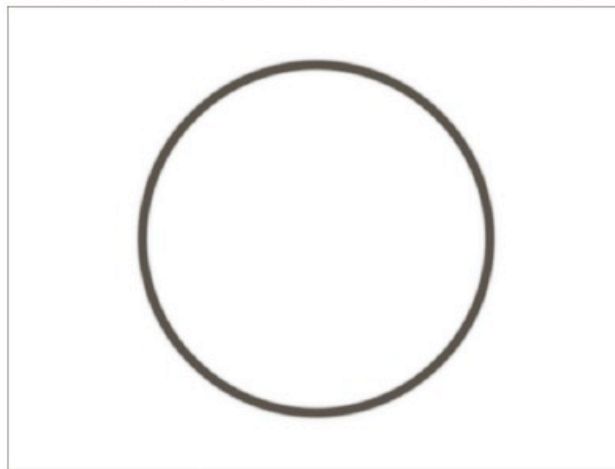
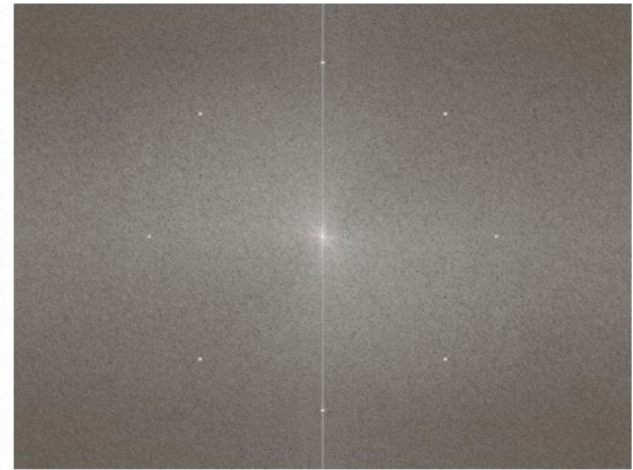
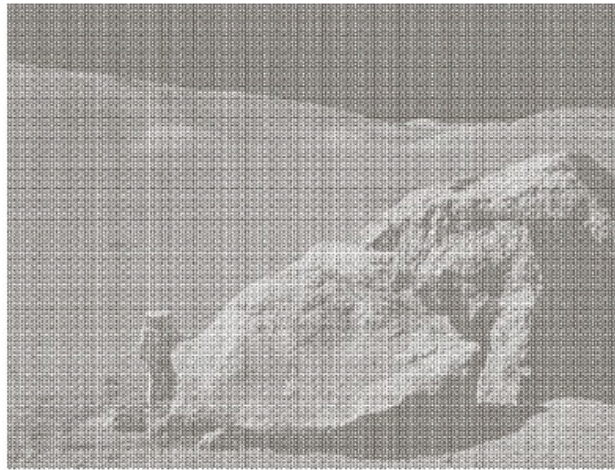
$$\hat{\tilde{f}}(\xi, \eta) = k(\xi, \eta) \hat{g}(\xi, \eta)$$

Bandreject filter

a	b
c	d

FIGURE 5.16

(a) Image corrupted by sinusoidal noise.
(b) Spectrum of (a).
(c) Butterworth bandreject filter (white represents 1).
(d) Result of filtering.
(Original image courtesy of NASA.)



Denoise methods

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- Variational approach

Variation approach-1

- Noise model: $z = u + n$ n : mean 0, variance σ^2

- Find a smooth solution u under constraint

$$\int |u - z|^2 = \sigma^2$$

- If the solution is to minimize H1 norm $\int |\nabla u|^2$
we call it H1 regularization

Variational approach to denoising-2

- H1 denoising $\min_u \int |u - z|^2 + \alpha \int |\nabla u|^2$

Euler-Lagrange equation

Regularization penalty

$$\alpha \Delta u - (u - z) = 0$$

- Total variation denoising $\min_u \int |u - z|^2 + \alpha \int |\nabla u|$

Euler-Lagrange equation

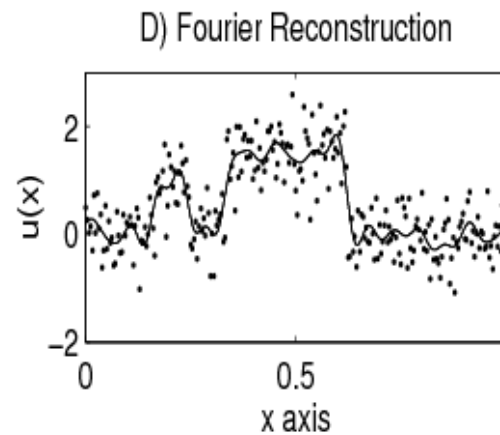
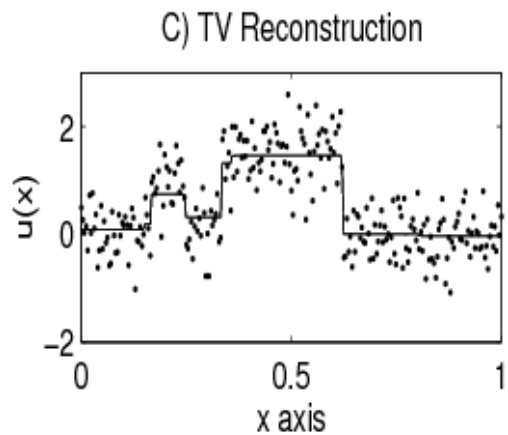
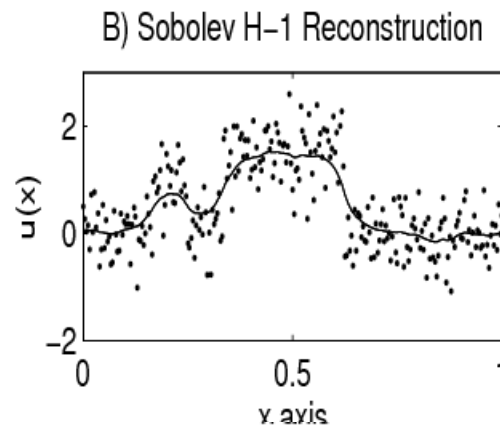
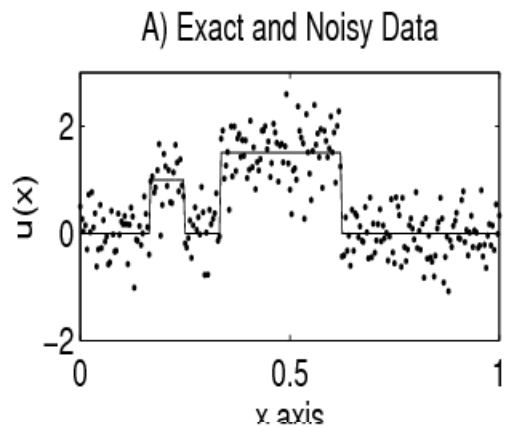
$$\alpha \nabla \cdot \left(\frac{\nabla u}{|\nabla u|} \right) - (u - z) = 0$$

Why Total variation denoising

- **TV norm: Keep edge sharp**

Rudin, Osher, Fatemi

TV norm is insensitive to jumps (edges)



Picture by Vogel and Oman

Image Processing

- What is Image?
- What is Image Enhancement?
 - Contrast Enhancement
 - Image Denoising
 - **Image Deblurring**
- Image Inpainting
- Image segmentation
- Image Registration

Book: Rafael C. Gonzalez and Richard E. Woods,
[Digital Image Processing](#), Prentice Hall

Blur model-1

- Convolution

$$g(x) = [h * f](x) := \int h(x - y)f(y)dy$$

- If h is a positive weight, then $h*f$ is an averaging process, i.e. blurring

- Example: Finite size mask $h_{s,t} = \frac{1}{16}$

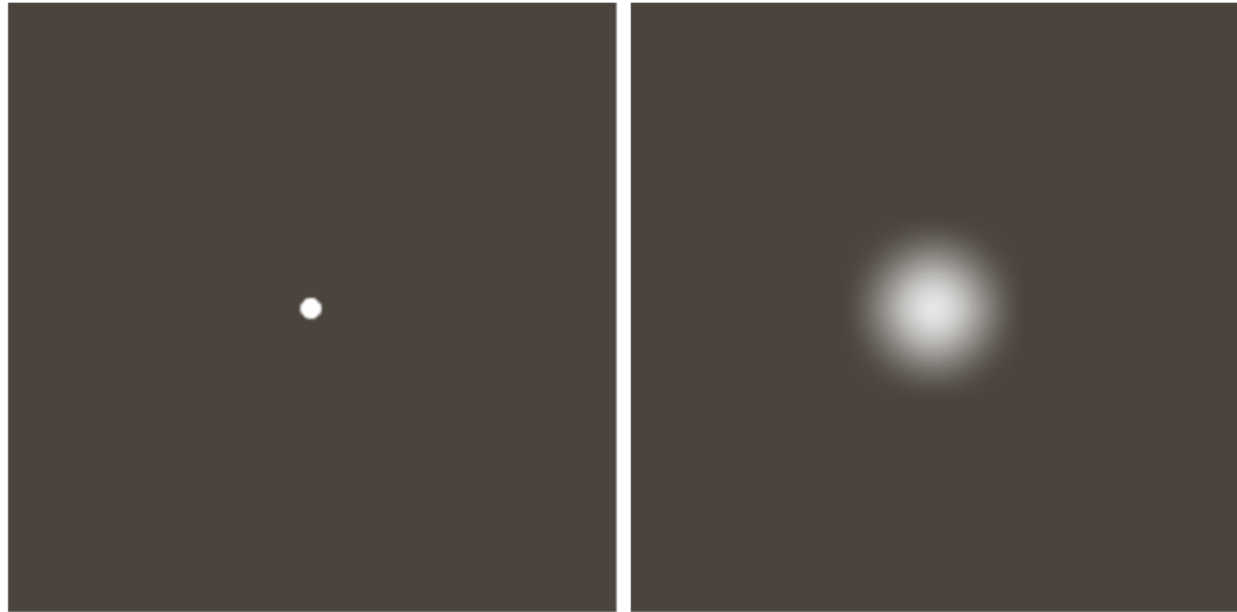
1	2	1
2	4	2
1	2	1

Blur model-2

a b

FIGURE 5.24

Degradation estimation by impulse characterization.
(a) An impulse of light (shown magnified).
(b) Imaged (degraded) impulse.



$$g = h * f$$

$$\hat{g} = \hat{h} \cdot \hat{f}$$

Atmospheric turbulence

$$\hat{h}(\xi, \eta) = e^{-k(\xi^2 + \eta^2)^{5/6}}$$

Gaussian model

$$\hat{h}(\xi, \eta) = e^{-k(\xi^2 + \eta^2)}$$

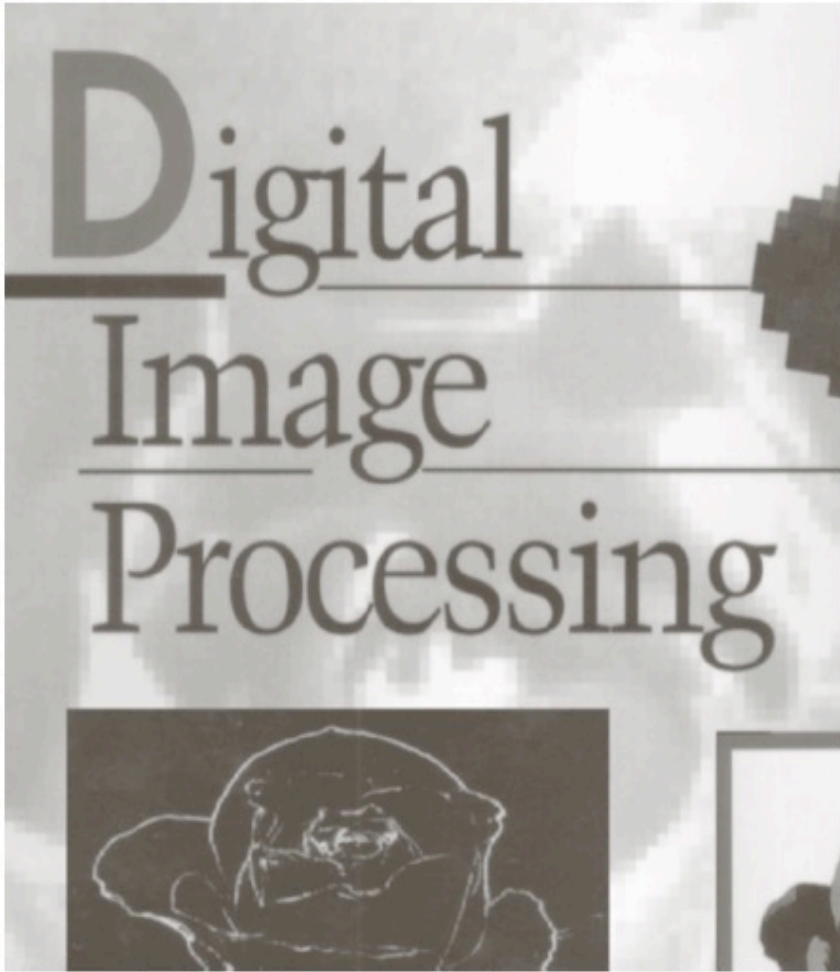
Blur model-3

a	b
c	d

FIGURE 5.25
Illustration of the
atmospheric
turbulence model.
(a) Negligible
turbulence.
(b) Severe
turbulence,
 $k = 0.0025$.
(c) Mild
turbulence,
 $k = 0.001$.
(d) Low
turbulence,
 $k = 0.00025$.
(Original image
courtesy of
NASA.)



Blur model -4



$$g(x, y) = \int_0^T f(x - x_0(t), y - y_0(t)) dt$$

K : Translation

Blur model-5

$$g = h * f + n$$

h: Blur operator

n: noise

f: true image

Deblur methods

- Deconvolution in frequency domain
 - Inverse filtering
 - Wiener filtering
 - ...
- Deconvolution via wavelets
- Variational approach

Deconvolution

$$\tilde{f} = k * g$$

- Inverse filtering

$$g = h * f + n \Rightarrow \hat{g} = \hat{h} \cdot \hat{f} + \hat{n}$$

$$\hat{\tilde{f}} = \hat{k} \hat{g} = \frac{1}{\hat{h}} \hat{g}$$

- Wiener filtering

$$\hat{k} = \frac{\overline{\hat{h}} E\{\hat{f}, \hat{f}\}}{|\hat{h}|^2 E\{\hat{f}, \hat{f}\} + E\{\hat{n}, \hat{n}\}}$$

Deblur-1



a b c

FIGURE 5.28 Comparison of inverse and Wiener filtering. (a) Result of full inverse filtering of Fig. 5.25(b). (b) Radially limited inverse filter result. (c) Wiener filter result.

Wiener filter

Deblur-2

Blur+noise

Inverse filter

Wiener filter



Deblur methods

- Deconvolution in frequency domain
 - Inverse filtering
 - Wiener filtering
 - ...
- Deconvolution via wavelets
- Variational approach

Deblur via TV regularization-1

- Blur model $g = h * f + n$

- Total variation regularization:

$$\min_f \alpha \int |\nabla f| + \int |h * f - g|^2$$

- Alternative formulation

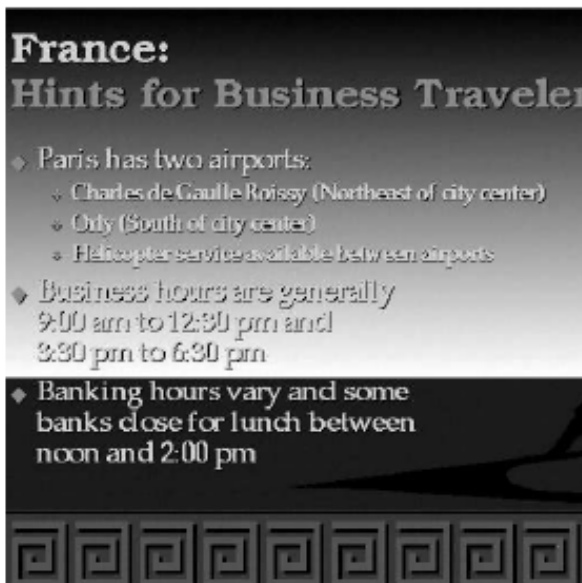
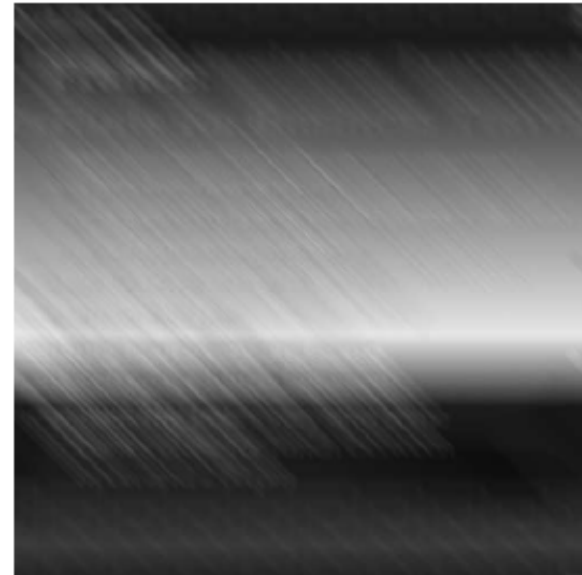
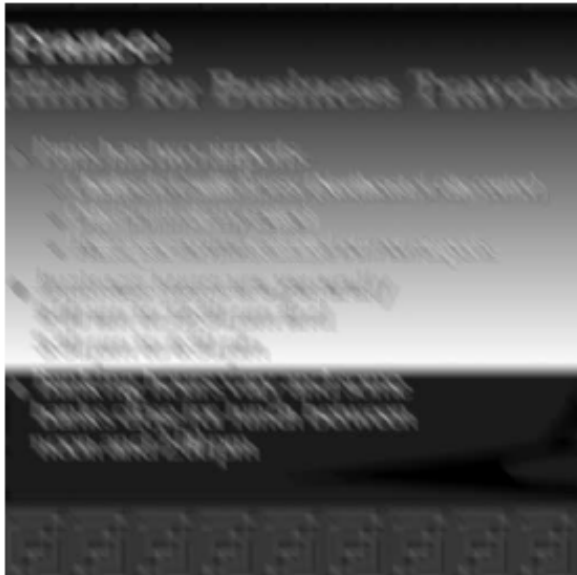
$$\min_{f,w} \alpha \int |w| + \beta \int |\nabla f - w|^2 + \int |h * f - g|^2$$

Deblur via TV regularization-2



Y Wang et al.

Deblur via TV regularization-3



Imaging Sciences

- **Image Acquisition (Imaging)**
 - human vision, Optics, Radar imaging, Ultrasound, MRI, X-ray CT,...

- **Image Processing**

$$I_{input} \xrightarrow{T} I_{output} = T[I_{input}]$$

- **Image Interpretation (Visual Intelligence)**

What is imaging?

- Use physical methods to get geometrical or physical properties of the objects
 - Geometry: shape, morphology, structure,...
 - Physical properties:
 - Mechanical: density, pressure, velocity, concentration, viscosity, diffusion coefficients,...
 - Electrical: potential, current, impedance, conductivity, resistance,
 - Optical: absorption/reflection...
 - nuclear

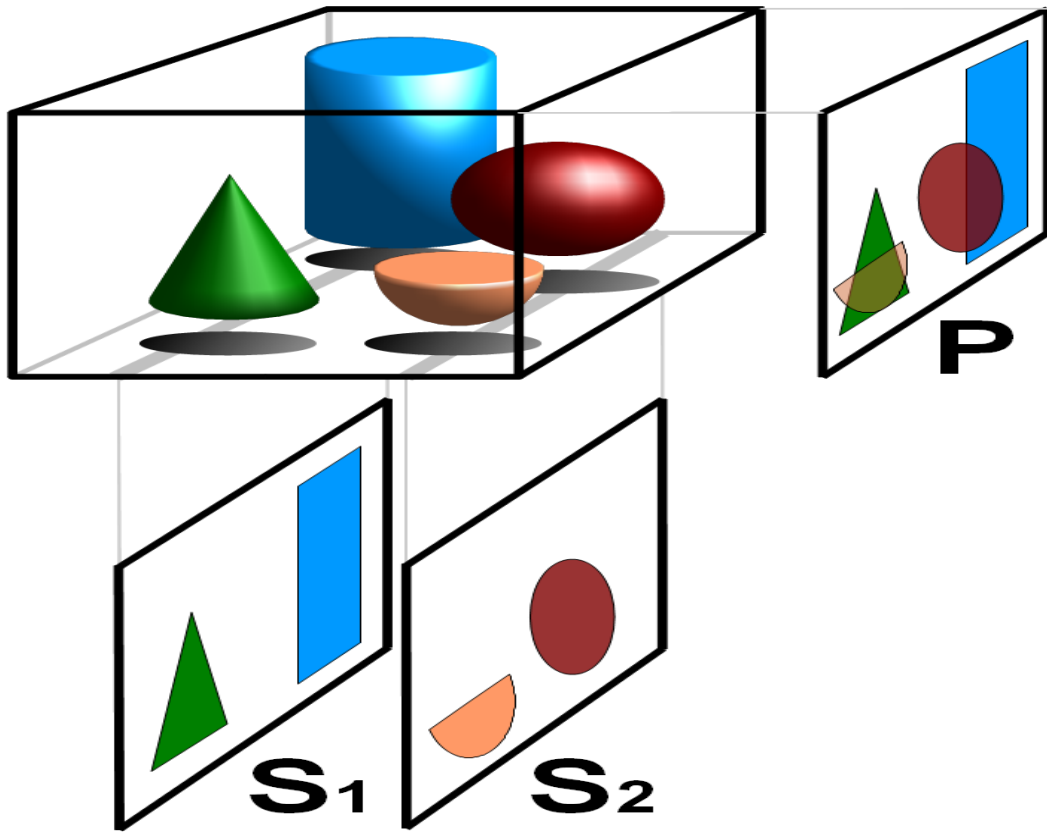
Medical imaging (Wiki)

- 1 Projection radiography
- 2 Tomography
- 3 Ultrasound
- 4 Fluoroscopy
- 5 Magnetic resonance imaging (MRI)
- 6 Nuclear medicine
- 7 Positron emission tomography (PET)
- 8 Photoacoustic imaging

Projection radiography



Tomography



Basic principle of tomography: superposition free tomographic cross sections S_1 and S_2 compared with the projected image P

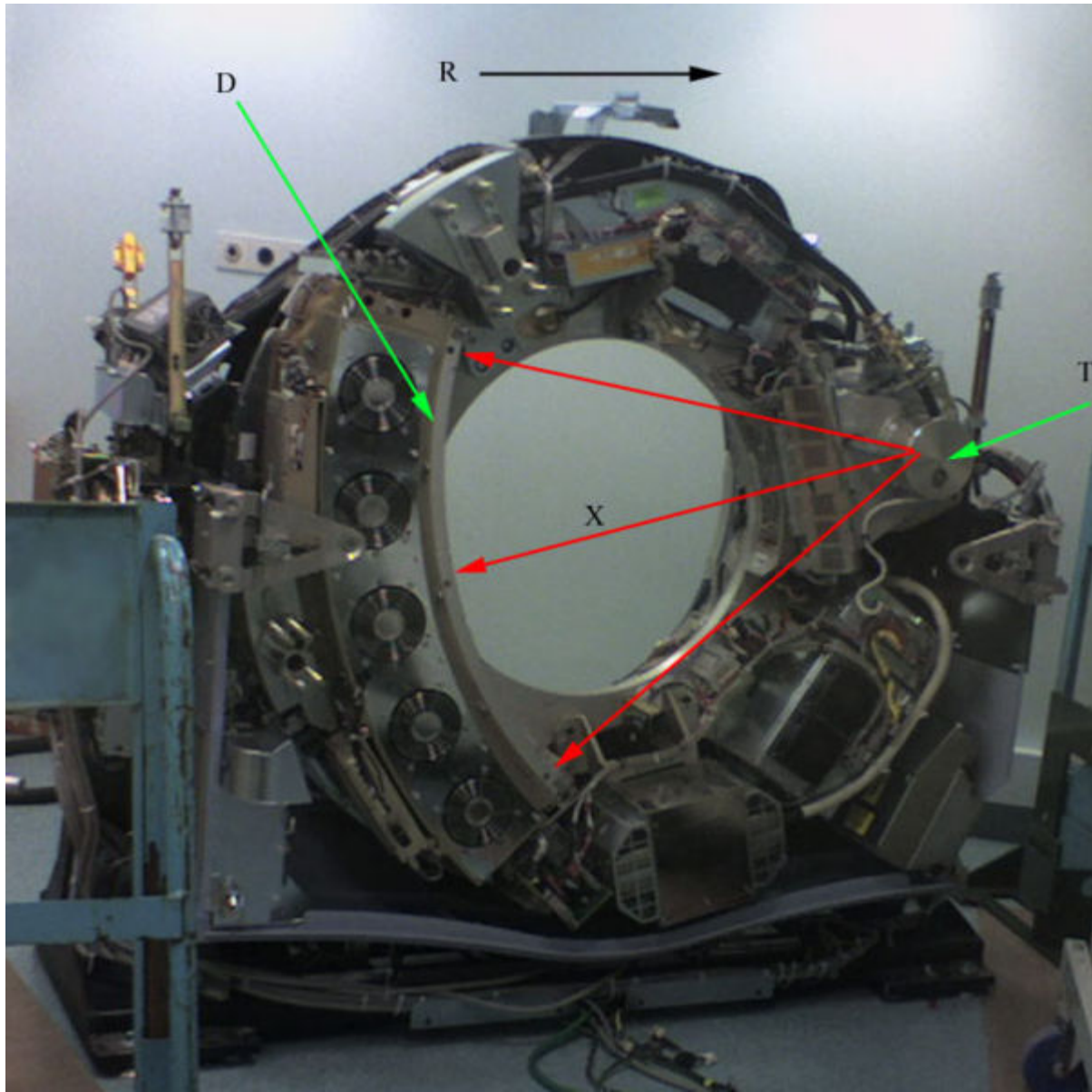
Type of Tomography-1

- Atom probe tomography (APT)
- Computed tomography (CT)
- Confocal laser scanning microscopy (LSCM)
- Cryo-electron tomography (Cryo-ET)
- Electrical capacitance tomography (ECT)
- Electrical resistivity tomography (ERT)
- Electrical impedance tomography (EIT)
- Functional magnetic resonance imaging (fMRI)
- Magnetic induction tomography (MIT)
- Magnetic resonance imaging (MRI), formerly known as *magnetic resonance tomography* (MRT) or nuclear magnetic resonance tomography

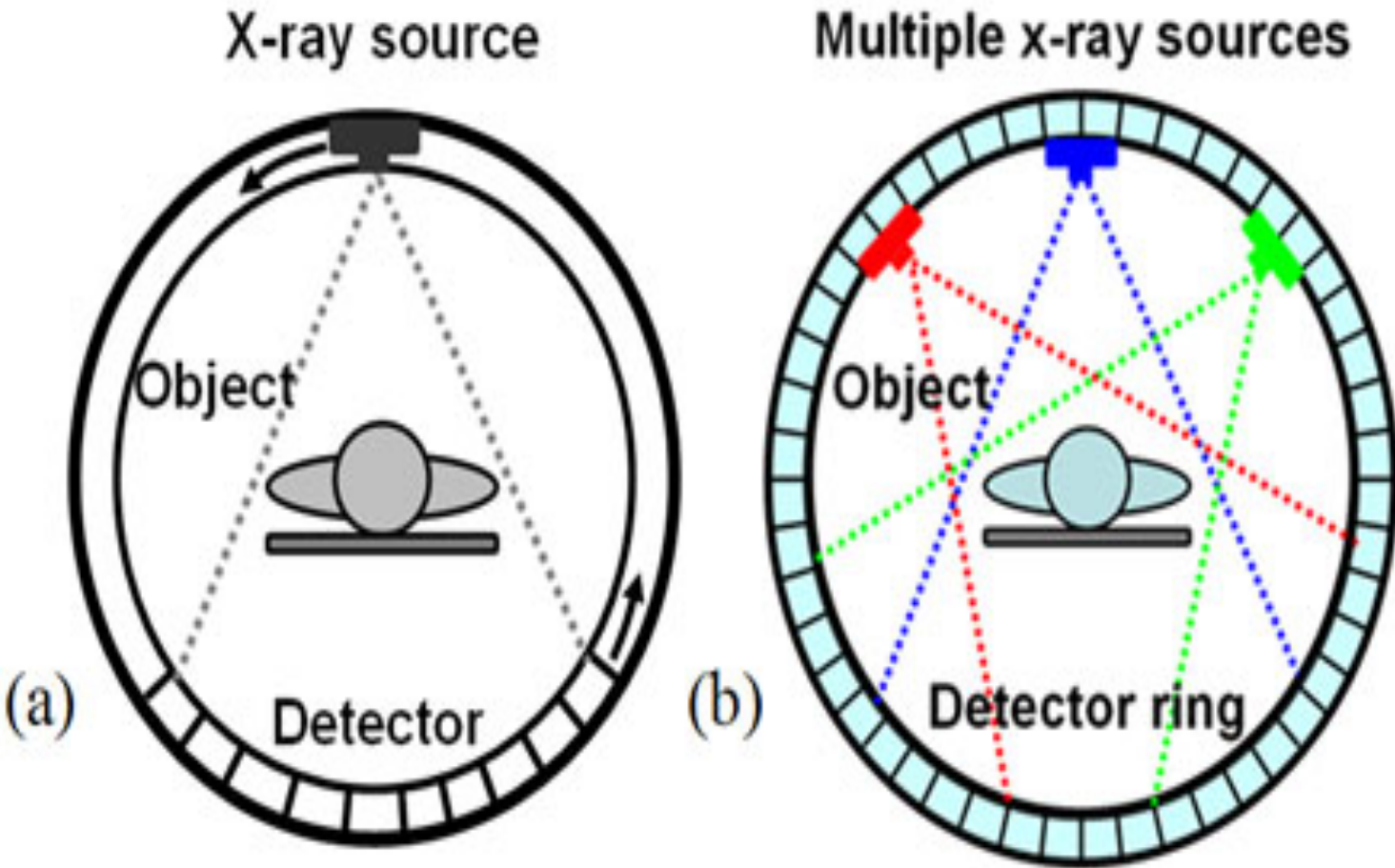
Type of Tomography-2

- [Optical coherence tomography](#) (OCT)
- [Process tomography](#) (PT)
- [Positron emission tomography](#) (PET)
- [Positron emission tomography - computed tomography](#) (PET-CT)
- [Quantum tomography](#)
- [Single photon emission computed tomography](#) (SPECT)
- [Seismic tomography](#)
- [X-ray tomography](#) (CT, CATScan)
- [Photoacoustic tomography](#) (PAT), also known as Optoacoustic Tomography (OAT) or Thermoacoustic Tomography (TAT)
- [Zeeman-Doppler imaging](#)

X-ray Computed Tomograph



X-ray CT



Nobel winners for CT (1979)



Godfrey Hounsfield



Allan McLeod Cormack

Image Reconstruction

- Tomographic reconstruction :

- Radon transform

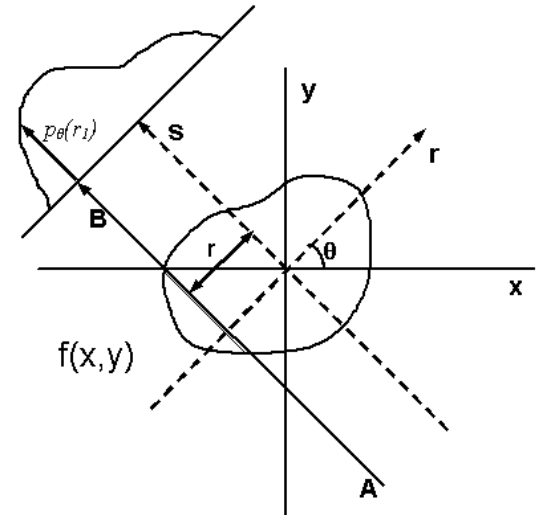
$$Rf(\theta, r) = \int_{x \cdot \theta = r} f(x) dx, \quad \theta \in S^1$$

- Imaging model

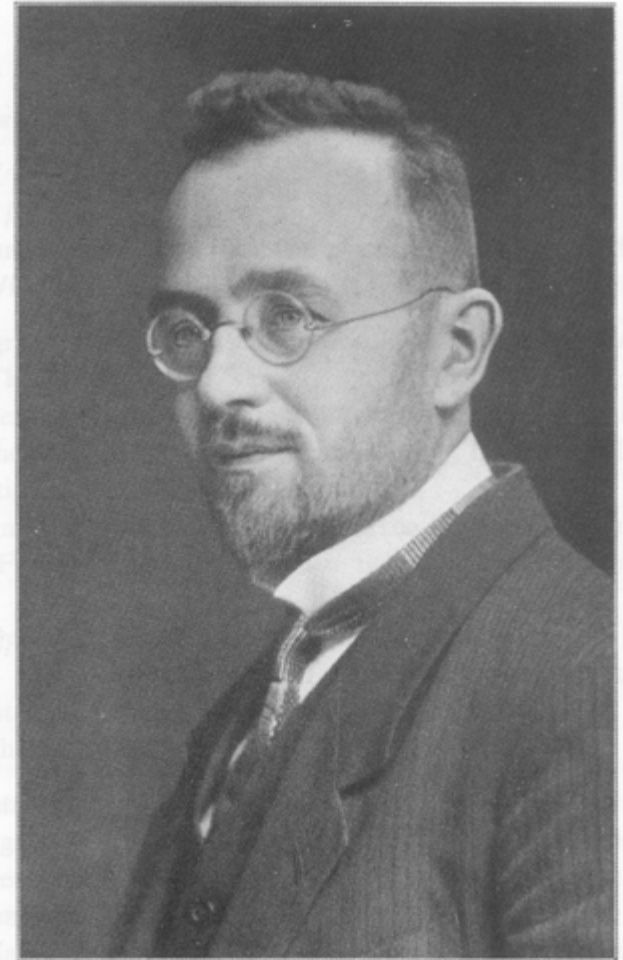
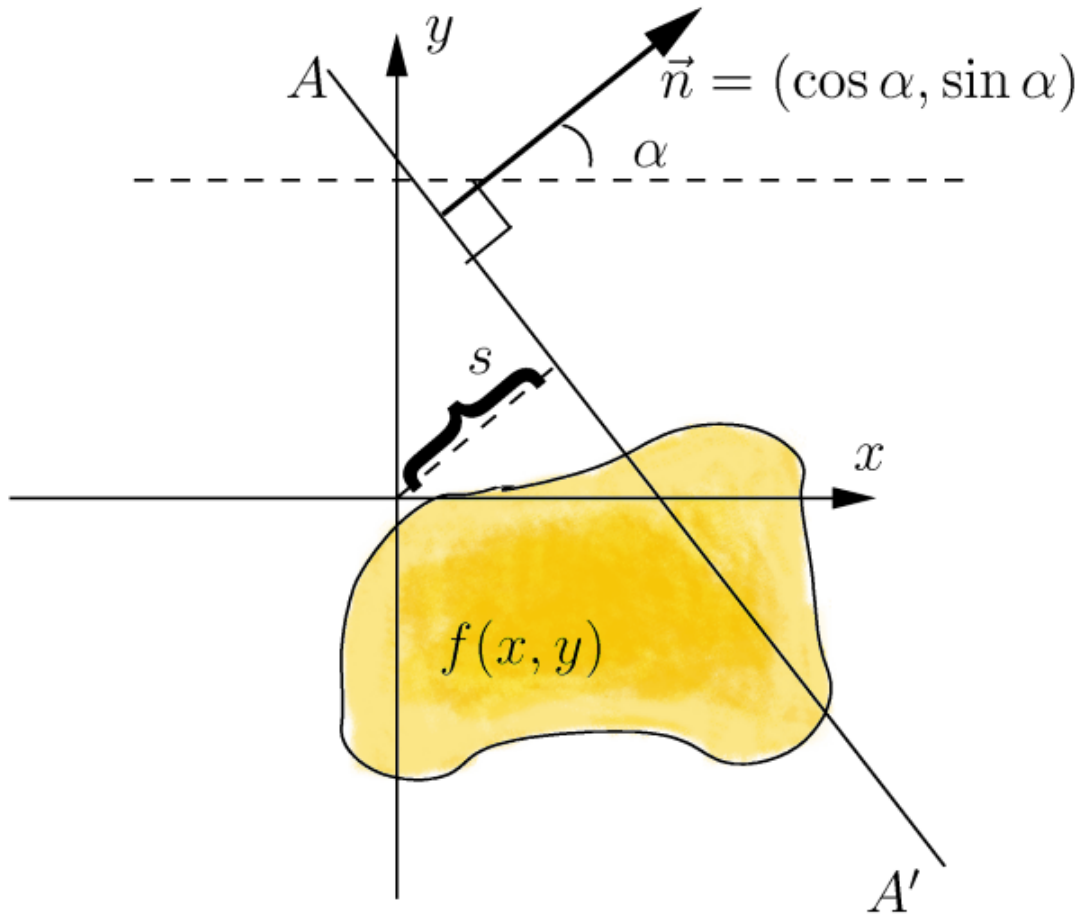
$$z = Ru + n$$

- Image reconstruction

Given z , reconstruct u

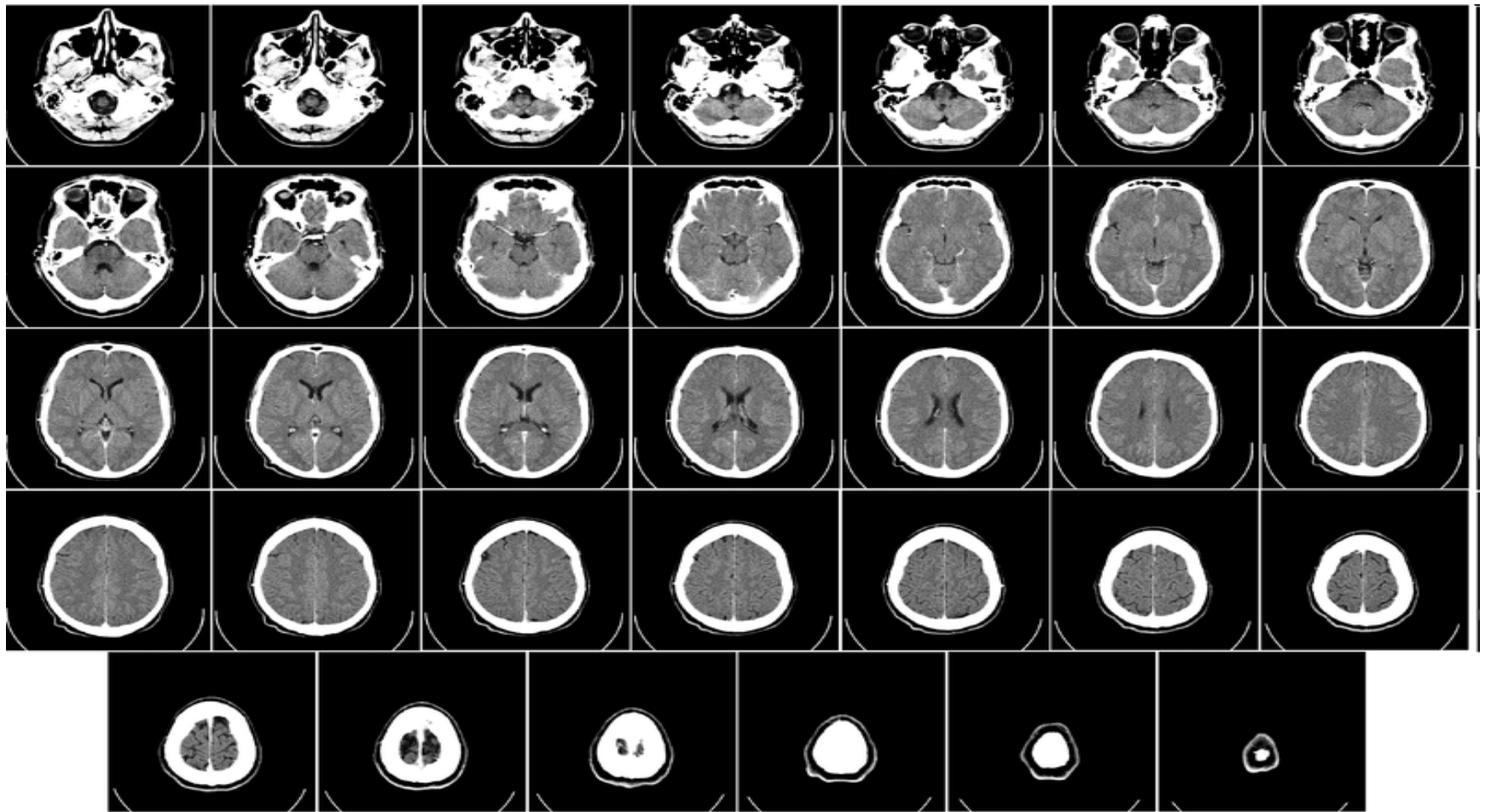


Radon transform

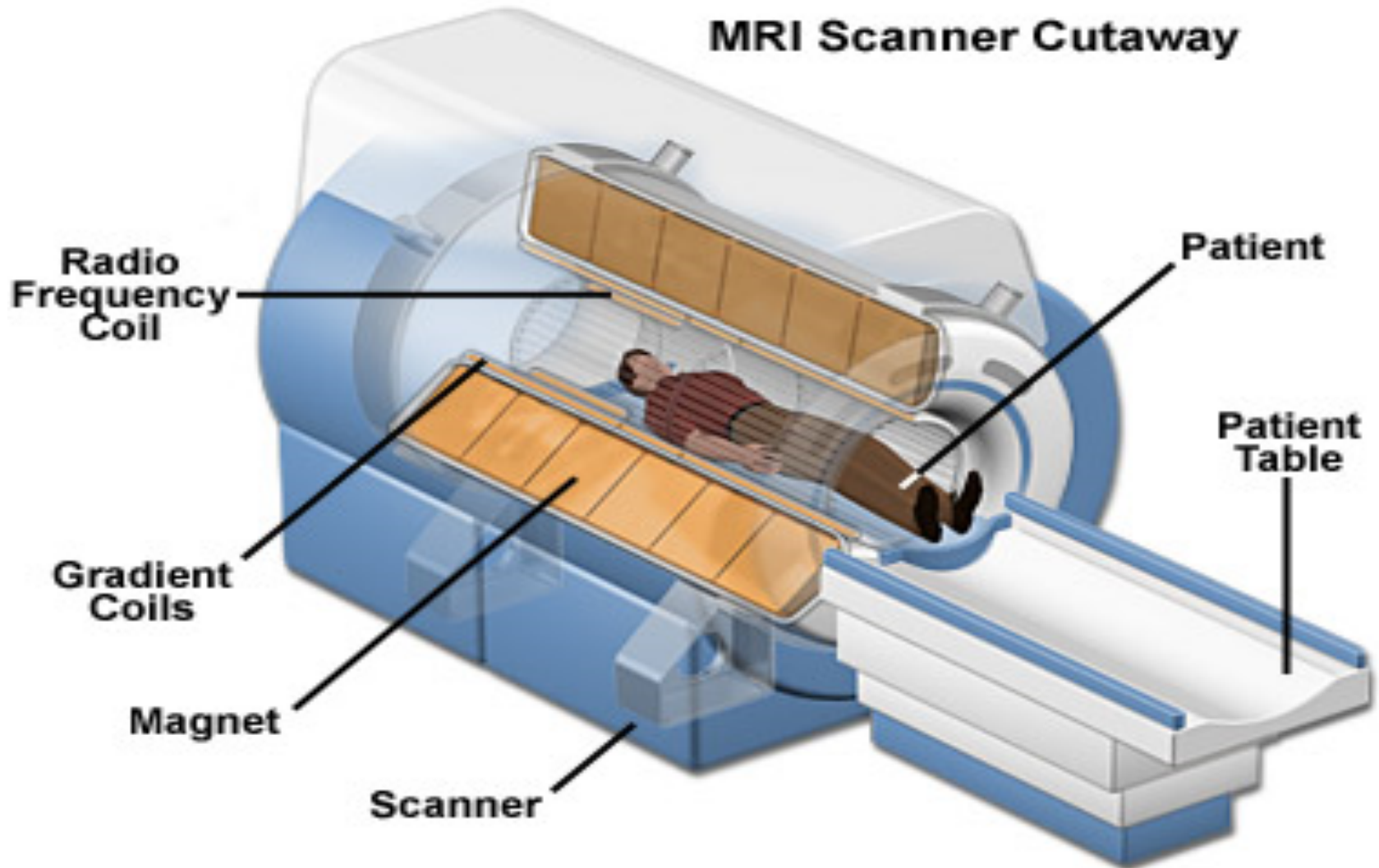


J. Radon

Reconstructed images by CT



Magnetic Resonance Imaging (MRI)



MRI history



The Nobel Prize in Physics 1952

"for their development of new methods for nuclear magnetic precision measurements and discoveries in connection therewith"



Felix Bloch

🕒 1/2 of the prize

USA

Stanford University
Stanford, CA, USA



Edward Mills Purcell

🕒 1/2 of the prize

USA

Harvard University
Cambridge, MA, USA



The Nobel Prize in Physiology or Medicine 2003

"for their discoveries concerning magnetic resonance imaging"



Paul C. Lauterbur

🕒 1/2 of the prize

USA

University of Illinois
Urbana, IL, USA



Sir Peter Mansfield

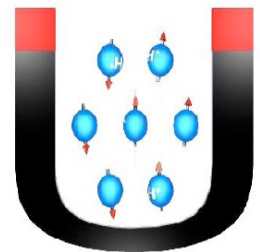
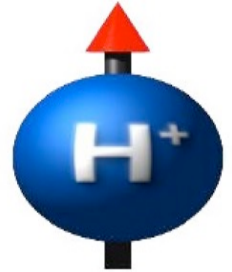
🕒 1/2 of the prize

United Kingdom

University of Nottingham,
School of Physics and
Astronomy
Nottingham, United
Kingdom

Basic Principles of Nuclear Magnetic Resonance

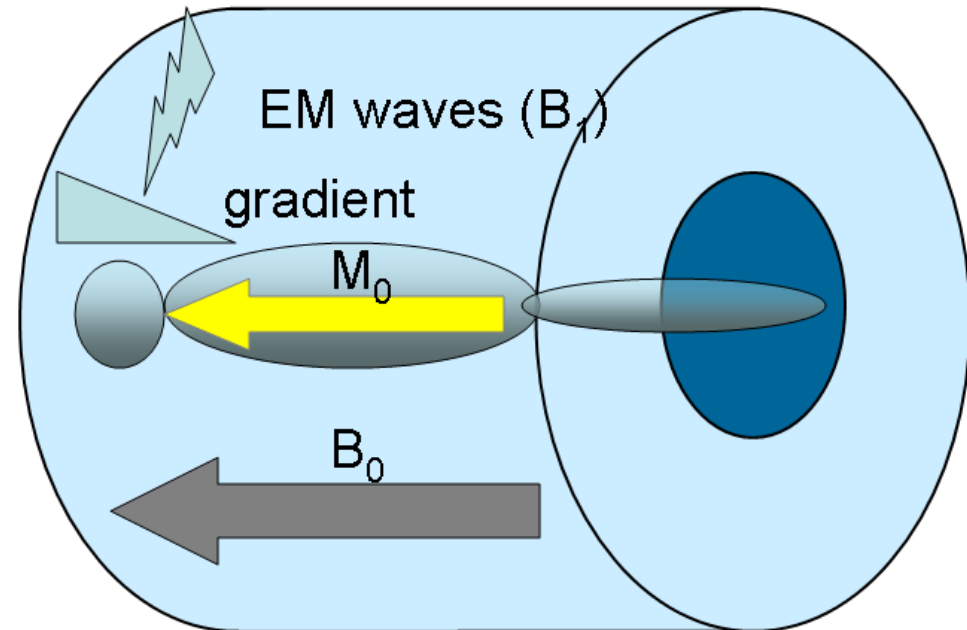
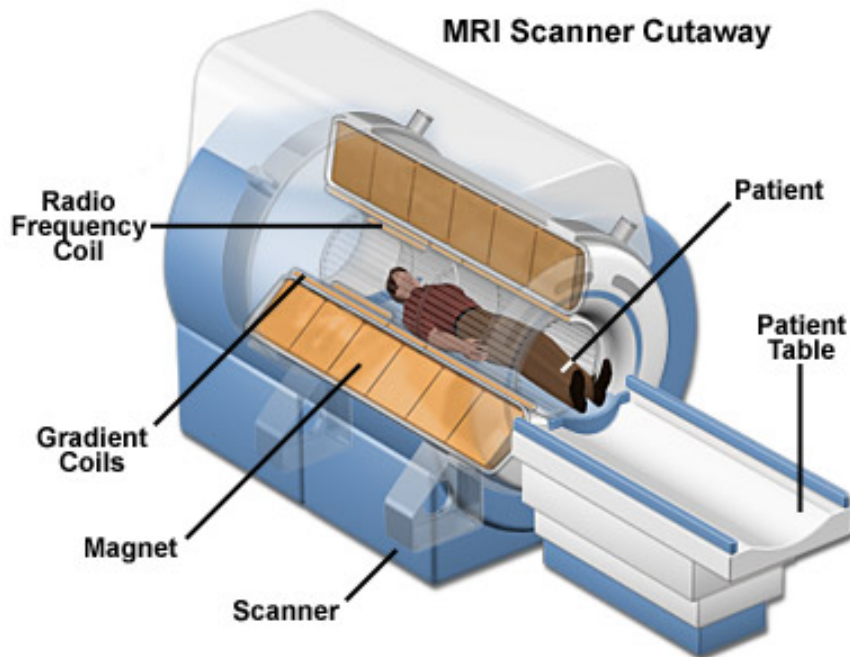
- Atoms with odd number of protons and/or neutrons possess nuclear spin angular momentum S
- Associated with S is a magnetic dipole moment
- Magnetic dipole moment rotates under external magnetic field, exhibit magnetic resonance phenomena
- The variation of rotation of spins generates magnetic fluxes and can be recorded
- Hydrogen H^+ atoms are abundant in biological specimens



MRI:

use magnetic fields to perform

- Relaxation: Main field B_0
- Excitation: Radio Frequency (RF) field B_1
- Fourier transform: Gradient field G

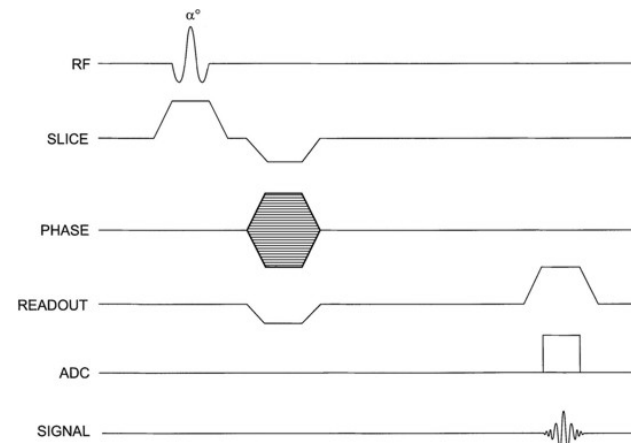
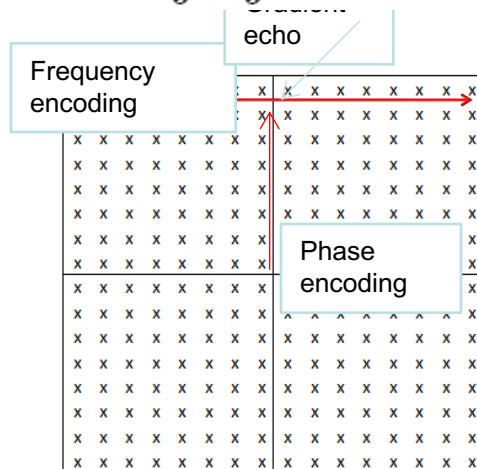


MRI is a Fourier integrator

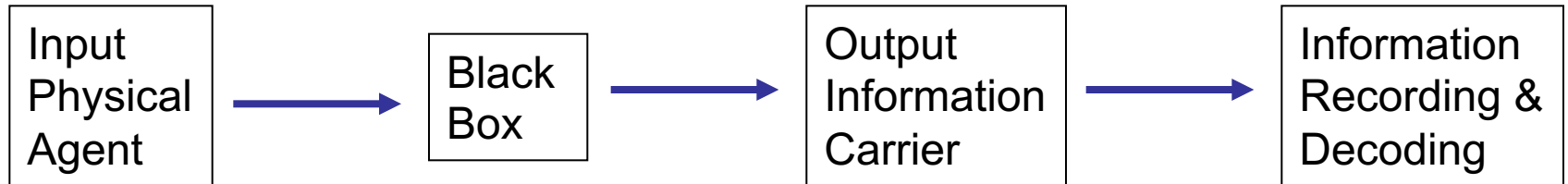
- RF excitation selects a slice of magnetic dipoles
- The gradient field generates Fourier transform of

$$s(t) = \int \int m(x, y) \exp \left(-i\gamma \int_0^t \mathbf{G}(\tau) \cdot \mathbf{r} d\tau \right) dx dy$$

$$= \int \int m(x, y) e^{-2i\pi [k_x(t)x + k_y(t)y]} dx dy$$



Magnetic Resonance Imaging



EM waves

Pulse sequences

Transmit coils

Contrast agents

Magnetic dipoles
of mobile protons

EM waves

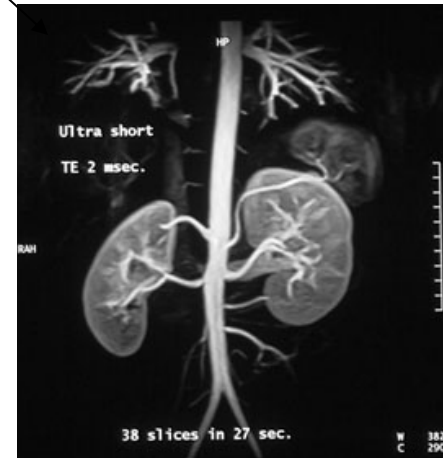
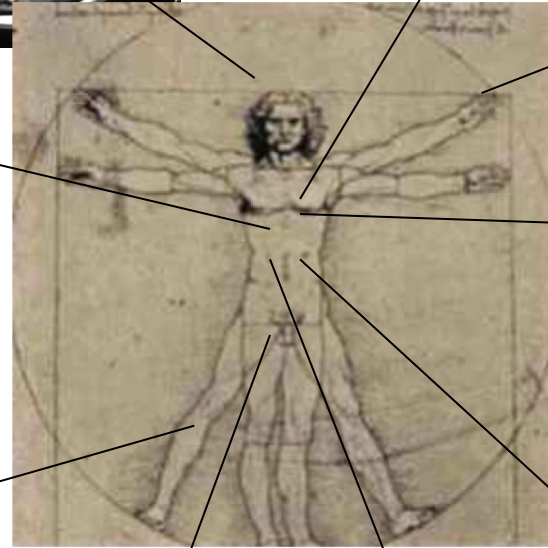
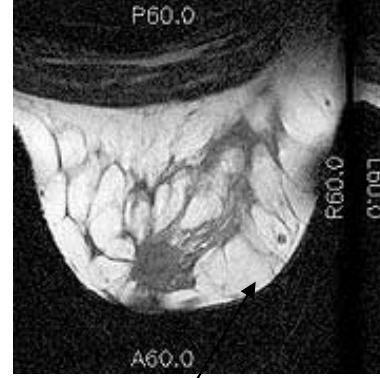
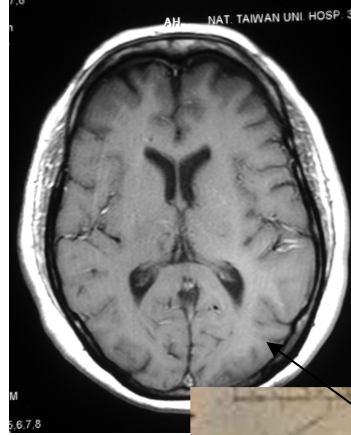
- T1 & T2
- Flow
- Diffusion
- Perfusion
- Temperature
- Cell tracking
- Molecules

Receive coils

Image reconstruction

Data processing

Data analysis



Summary of Imaging Sciences

- Imaging (data acquisition): CT, MRI
 - Solving inverse problems
- Image processing:
 - Enhancement (contrast enhancement, denoising, deblurring,...)
 - Segmentation (edge detection, active contours,...)
- Image analysis, image interpretation

Image science and mathematics

- Image science is important in medicine
- Low dose, high resolution imaging methods are needed
- Image science needs mathematics

- Thank you for your attention.